

QUANTUM INFORMATION

A molecular quantum spin network controlled by a single qubit

Lukas Schlipf,^{1,2} Thomas Oeckinghaus,² Kebiao Xu,^{1,2,3} Durga Bhaktavatsala Rao Dasari,^{1,2} Andrea Zappe,² Felipe Fávoro de Oliveira,² Bastian Kern,¹ Mykhailo Azarkh,⁴ Malte Drescher,⁴ Markus Ternes,¹ Klaus Kern,^{1,5} Jörg Wrachtrup,^{1,2} Amit Finkler^{2*}

Scalable quantum technologies require an unprecedented combination of precision and complexity for designing stable structures of well-controllable quantum systems on the nanoscale. It is a challenging task to find a suitable elementary building block, of which a quantum network can be comprised in a scalable way. We present the working principle of such a basic unit, engineered using molecular chemistry, whose collective control and readout are executed using a nitrogen vacancy (NV) center in diamond. The basic unit we investigate is a synthetic polyproline with electron spins localized on attached molecular side groups separated by a few nanometers. We demonstrate the collective readout and coherent manipulation of very few (≤ 6) of these $S = 1/2$ electronic spin systems and access their direct dipolar coupling tensor. Our results show that it is feasible to use spin-labeled peptides as a resource for a molecular qubit-based network, while at the same time providing simple optical readout of single quantum states through NV magnetometry. This work lays the foundation for building arbitrary quantum networks using well-established chemistry methods, which has many applications ranging from mapping distances in single molecules to quantum information processing.

INTRODUCTION

Coherent control over a many-qubit system, as well as readout of few or single elementary qubits within this system, is key for quantum information processing techniques. Among the different realizations of qubits, electron and nuclear spins in solids show unprecedented coherence times of up to 6 hours (1), can be coherently controlled at gigahertz rates (2), and read out optically (3) as well as electronically (4). However, scaling of, for example, spin systems to larger regular arrays is a daunting technical task because typical distances for coupling electron spins via magnetic dipole interaction [below 30 nm (5)] are currently out of reach for reliable top-down nanotechnology. However, a programmable molecular structure can very well cover these length scales (6, 7), for example, using sequence-controlled self assembly of peptides on surfaces (8). These systems show a high degree of regularity required for complex patterns, which are built up from simple, interacting quantum systems. In addition, their flexible chemistry allows them to be manipulated into virtually any shape, such that their design can adopt various spin lattices in two and three dimensions (9, 10). Here, we demonstrate measurement of a small basic unit cell for the goal of providing both scalability and a mechanism for quantum information readout, comprising two electron spins positioned on a molecule. Probing the coupling between the two spins and ultimately driving them in a coherent fashion constitute an essential building block for a molecular spin network.

Quantum spin networks are known to integrate and scale up quantum registers involving many qubits. Combined with local control in implementing quantum logic gates, spin chains can greatly facilitate large-scale quantum information processing (11–13). In addition to

the naturally available spin chains in materials (14), artificial spin chains are realized with quantum dots (15), chains of magnetic atoms (16), Josephson junction arrays (17), and trapped ions (18). Although the spin-spin distances in materials range in the 10-nm regime, offering scalability and high coupling strength among nearest neighbors, they are less controllable even at the few-spin level. On the other hand, artificially formed spin chains are more controllable, allowing them, for example, to be used as simulators for understanding energy transport in complex networks (19). In the intermediate regime of length scales in the nanometer region, molecular chemistry offers stable scaffolds to build scalable spin networks. These systems have mostly been studied in the context of magnetic resonance for distance measurements among the spins (20) but typically in the ensemble limit of around 10^9 spins due to sensor limitations. Therefore, it is necessary to find a suitable sensor system that can read out quantum information from this spin network on the local scale of a few spins in a non-invasive fashion.

Over the past few years, a novel atom-sized defect in the form of a nitrogen vacancy (NV) center in diamond has revealed the ability to perform magnetic resonance studies on very few spins in a nanoscale volume (21, 22), wherein its quantum nature is harnessed for magnetometry using optical means. Quantum-limited sensitivity has been achieved using the NV center in detecting single electron (23, 24) and nuclear spins (25, 26) external to the diamond lattice. Its long coherence time (27), even in close proximity to the surface, makes it possible to sense a single electron spin at a distance more than 30 nm from the NV center (28). This unique atomic-sized defect serves here as a probe for a network's unit cell, reading it out with high fidelity using confocal microscopy, while microwave pulses facilitate manipulation of the sensor and network spins.

RESULTS

We choose a synthetic, proline (P)-rich peptide as a spacer model system, $\text{H-AP}_{10}\text{CP}_{10}\text{NH}_2$, containing two cysteine (C) amino acids at specific positions, to which various spin labels can be easily attached

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¹Max Planck Institute for Solid State Research, Heisenbergstraße 1, 70569 Stuttgart, Germany. ²Physikalisches Institut, Universität Stuttgart, Pfaffenwaldring 57, 70569 Stuttgart, Germany. ³Chinese Academy of Sciences Key Laboratory of Microscale Magnetic Resonance and Department of Modern Physics, University of Science and Technology of China, Hefei 230026, China. ⁴Department of Chemistry, Zukunftskolleg, and Konstanz Research School Chemical Biology, Universität Konstanz, Universitätsstraße 10, 78457 Konstanz, Germany. ⁵Institut de Physique, École Polytechnique Fédérale de Lausanne, 1015 Lausanne, Switzerland.

*Corresponding author. Email: a.finkler@physik.uni-stuttgart.de

via site-directed spin labeling (SDSL). Because of the relatively high stiffness of the proline backbone (29, 30), the electron spins attached to the polyproline (network spins) are well localized, making them resilient to phonon-induced decoherence, even at finite temperatures. These network electron spins are locally probed and controlled by their dipolar coupling to the close-by electron spin located on the NV center in diamond (probe spin). To enable this coupling, we use shallow NV centers close to the diamond surface (<10 nm), on which we deposit the spin-labeled peptides (Fig. 1A). The higher gyromagnetic ratio of the network electron spins in comparison to nuclear spins makes it more feasible to drive coherent oscillations at high frequencies and detect their response (31).

The sensor spin, namely, the NV center, is a ground-state paramagnetic $S = 1$ spin system, which can be optically polarized with near unit efficiency to the nonmagnetic ($m_z = 0$) ground state of the spin. Similarly, its spin-state projection on its quantization (z) axis can also be read out optically with high fidelity (3). Because of a relatively large zero-field splitting of the NV center, its spin-state manipulation by microwave fields can be quite different from the network electron spins (2), enabling independent control. To efficiently characterize the spin network on the nanoscale using the NV center spin-state readout, our first goal is to unravel the various couplings involved in the dynamics. For this, we use double electron-electron spin resonance techniques (see Materials and Methods) as detailed in the following.

Here, we choose the common methanethiosulfonate spin label (MTSSL) as a network spin, which will lead to three distinct hyperfine spectral peaks because of the hyperfine coupling of its electronic $\sigma = 1/2$ spin from an oxygen radical with a next-neighbor ^{14}N nuclear spin (total spin quantum number $I = 1$) (24). Initially, we cover the diamond containing the NV center with MTSSL-bearing peptides (see Materials

and Methods). Using this sample preparation, almost every NV center shows a strong electron spin signal peak (see the Supplementary Materials). Although it is likely that ≥ 50 spins are detected, spectra showing two distinct side peaks under ambient conditions can be found. This behavior is attributed to motional narrowing of the different inhomogeneous spectra because peptides were not immobilized on the diamond surface, and hence, molecular tumbling can be significant (32).

One well-known problem in optical excitation of organic molecules is photobleaching, that is, chemical reactions and the accompanying structural and electronical changes induced by supplying energy in the form of photons. Typically, around 1 mW of power is focused on a diffraction-limited spot to saturate the NV center fluorescence. Because of this, the electron spins within a dipolar coupling range to the NV center also experience a power density of usually $10^9 \text{ W} \cdot \text{cm}^{-3}$, which can often lead to a change or loss of the electronic spin properties in the molecule. We observe a bleaching of the MTSSL electron spin contrast on an hour time scale in almost all cases, preventing more elaborate experiments. To extend this time scale, often lowering the temperature of the system under investigation (33) and stripping the environment of oxygen to prevent photocatalytic reactions are of great benefit. Consequently, all of the following experiments were conducted at liquid helium temperatures (4.2 K) and in a UHV environment ($p < 10^{-8}$ Pa) (34), wherein we do not observe photobleaching of the organic network spins, demonstrated by an excellent signal stability.

Upon cooling the dense network spin sample we described above, the previously observed narrow lines uniformly show significant broadening (Fig. 1C). This can be explained by the freezing out of any network spin motion on the time scale of the measurement and

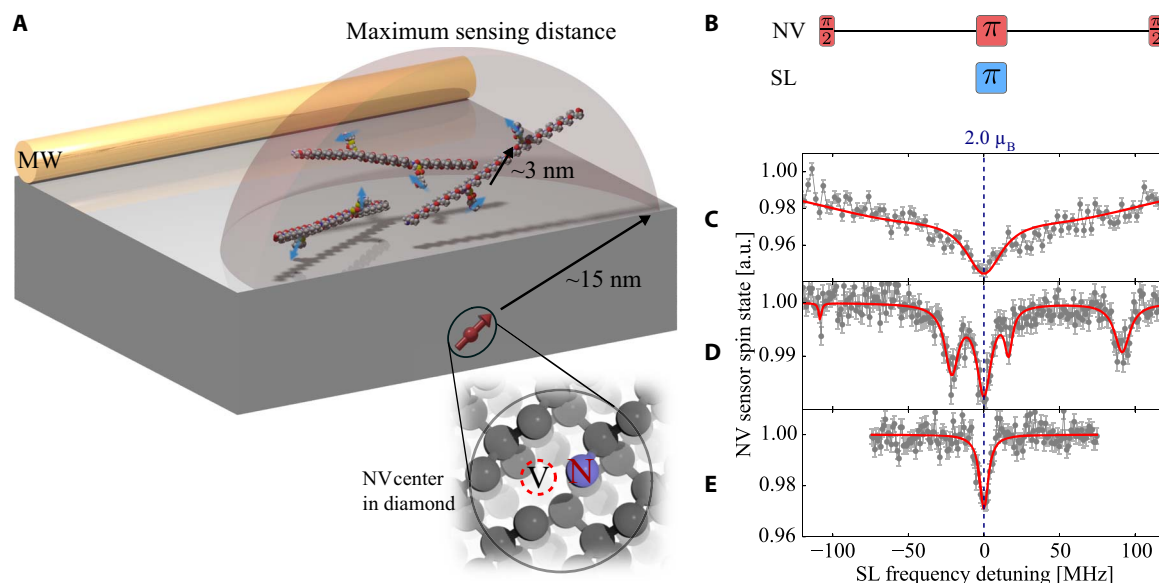


Fig. 1. Spectroscopy of few spin-labeled peptides. Electron spin spectra measured at $T = 4.2$ K and ultrahigh vacuum (UHV); (A) Experimental sketch: The shallow NV center spin couples to doubly spin-labeled polyprolines. Coherent control over all participating spins is provided by a close-by ($\sim 50 \mu\text{m}$) microwave wire (MW). The edge of the depicted sphere is the maximum sensing radius for a single electron spin to be detected, delimited by the NV centers' T_2 time. The intrapeptide coupling is almost two orders of magnitude larger than any of the other couplings in the few-peptide case, especially the interpeptide coupling. (B) Pulse sequence used to probe the spectrum of external network spins. Red pulses address the NV center spin, whereas the frequency of the blue pulse is swept to address network spin labels (SL). (C) Measured spectrum on a diamond membrane coated exclusively with spin-labeled peptides. The fit of the spectrum is a numerical simulation over random orientations of 50 MTSSL spin labels, including decoherence effects due to interpeptide couplings. a.u., arbitrary units. (D) Same as (C) but the labeled polyprolines were diluted with unlabeled ones at a ratio of 1:10. Distinct hyperfine couplings are clearly visible. (E) Measurement of a diamond dangling bond dark spin on a cleaned membrane for comparison.

the resulting loss of motional narrowing. In this case, the resulting spectrum can be well described by a sum over all possible orientations. The high network spin density has a great effect on the coherence of the electronic network spins due to electron-electron flip-flop processes, while at the same time, the magnitude of sensor-network couplings makes it impossible to access single-network spin states. Therefore, we reduced the sensor-network coupling to only a few spins.

To this end, we diamagnetically dilute the peptide stock solution using nonlabeled peptides with a ratio of 1:10 before deposition on the diamond surface, increasing the interpeptide spin-spin distance in the resulting homogeneously mixed molecular film. Subsequently, we observe spectra on NV centers with narrow peaks at low temperature (Fig. 1D), suggesting low spin-spin interaction between the network spins and thus probe-to-network coupling with only a few participating spins, as depicted in Fig. 1A. Because of the rather high concentration of spin-labeled molecules, the ratio of NV centers exhibiting broad peaks to narrow peaks was approximately 40:1. We select an NV center showing four distinct side peaks (Fig. 1D) for all following measurements, possibly caused by pairs of electron spins at different angles and positions, which is expected from a few peptides in the sensing volume. To maximize signal intensity and access all directions at the same time in the following, we drive the external spins on the central peak at zero detuning (dashed blue line in Fig. 1E), which is independent of spin label orientation.

By fixing the π pulse transition frequency at any of the hyperfine peaks, we vary the application timing τ of the network spin pulse within the sequence (Fig. 2A) or equivalently vary the total length of the sequence. With this and various sensor-to-network couplings F^k involved, the resulting population difference among the probe spin states C_{NV} oscillates as

$$C_{\text{NV}}(\tau) = \frac{1}{2} \left[1 + \prod_k^M \cos(F^k \tau) \right]$$

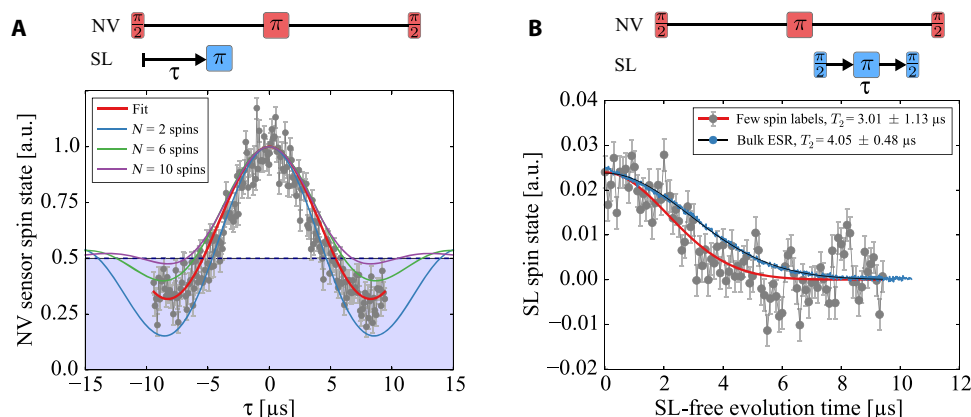


Fig. 2. Coupling to only few MTSSL spin-labels. (A) Coherent oscillation due to dipolar couplings between sensor and network spins, clearly visible by contrast inversion (blue shaded area) of the NV probe spin state, which suggests a low number of participating network spins. For the measurement, we choose a constant evolution time of 19.8 μs for the NV probe spin Hahn echo sequence, maximizing interaction time. Previous to the measurement, $T_2 = 14.0$ μs of the NV center under investigation was measured. To access the coupling between sensor and network spins, we sweep the application point of the network π pulse within the free evolution of the sensor spin coherence. The measurement data are accompanied by simulations of coupling strength oscillations caused by $n = 2, 6$, and 10 randomly distributed spins above the diamond surface. We would like to stress that it is difficult to estimate the precise number of spins here, and the relative strength of the overshoot below the NV sensor mixed state (0.5) heavily depends on the couplings (positions) of the participating network spins. (B) Hahn echo measurement on the external network spins directly probing their T_2 time via the readable signal from the probe spin (red). The blue curve was measured on a pulsed EPR spectrometer at 10 K in a frozen solution of water/glycerol (4:1) using the same peptides. A low concentration guarantees a proper separation between peptides, and the agreement of both coherence times points toward comparable SDSL peptide-peptide distances in both samples.

we use a third radio frequency (RF) to address different network spins simultaneously. Accordingly, it seems naturally conclusive to perform a decoupling sequence on the network spins themselves while sweeping a third π pulse and investigate its effect on the coherence created on the network spins (Fig. 3, A and B). This, in principle, amounts to addressing two external spins separately by two distinct RF frequencies.

However, because the coupling is small and the width of the RF pulses is non-negligible in our case, this triple-resonance scheme is sensitive to the interspin coupling of the network spins as

$$C_{\text{NV}}(\tau) \sim 1 - \prod_k^M \sin^2(F^k \tau) \cos(J^{\parallel} \tau) \cos(J^{\perp} \tau)$$

even when driving the network decoupling sequence at the Larmor frequency of the network spins and having a substantial overlap of the

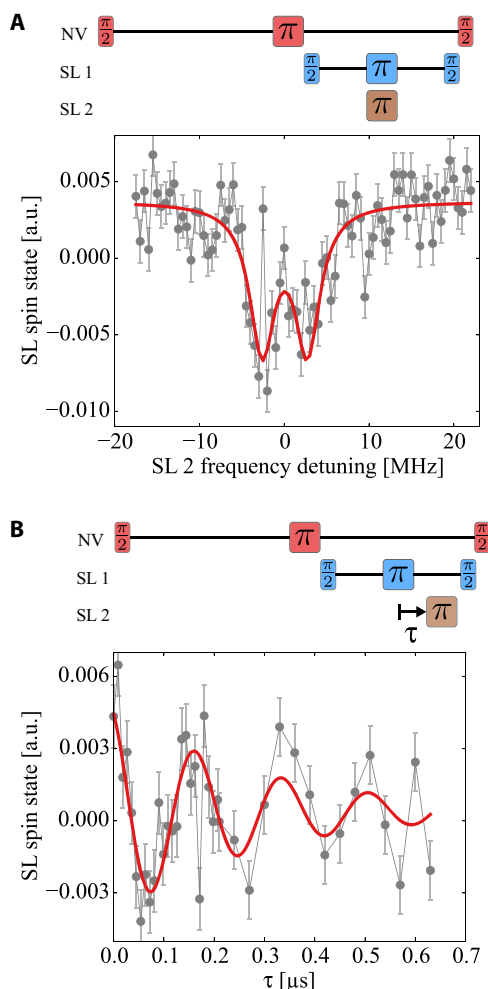


Fig. 3. Access to dipolar coupling between MTSSL spins. (A) Measurement of a triple-resonance frequency sweep on a few network spins (Figs. 1D and 2) with a π pulse width of 3.4 MHz. The swept frequency channel is SL 2, whereas SL 1 is kept at zero detuning to create a coherent superposition. The resulting spectrum can be fitted with two Lorentzians (red), as is expected from a pronounced J coupling between network spins. (B) Delay measurement on a the same environment, where we fix the excitation frequency of SL 1 at the network Larmor frequency and the SL 2 sweeping π pulse frequency 3 MHz apart from it. The red curve is a fit using a decaying cosine. The oscillations reveal the very same coupling strength as the frequency sweep in (A).

excitation pulses (see the Supplementary Materials). Here, the coupling between network spins is described by a parallel $J^{\parallel}$ and a perpendicular $J^{\perp}$ term (see Materials and Methods). We would like to stress that a proper choice of the excitation frequencies here can give access to the different elements of the dipolar coupling tensor.

We apply the triple-resonance scheme to the previously investigated NV center probe environment. Here, the decoupling of the network spins is performed at their Larmor frequency while sweeping the frequency of a third π pulse. The resulting spectrum is plotted in Fig. 3A and shows two distinct peaks, with an effective coupling strength of 5.2 ± 1.0 MHz. To support these findings, we fix the second excitation frequency at the right peak and sweep the delay within the decoupling sequence, as we did to determine the probe-network coupling. Using this sequence, the intracell coupling is probed, and accordingly, the result is a distinct oscillation, shown in Fig. 3B, with a frequency of 5.8 ± 1.0 MHz, which is in agreement with the previous measurement. Both measurements are supported by numerical simulations, reproducing the behavior for a J -coupled spin system probed by the NV spin sensor (see the Supplementary Materials). Furthermore, we have performed control measurements, driving one of the two excitation channels far off-resonance to exclude any microwave artifacts, and did not observe any coupling. In addition, we conducted measurements on a freshly cleaned sample with different electron spin systems, which did not show any hyperfine interaction (Fig. 1E). These are most likely dangling bonds on the diamond surface and therefore not expected to exhibit any distinct dipolar coupling because their positions on the diamond surface are random. This was likewise not observed in our experiment.

DISCUSSION

We have shown coupling of a single NV center spin sensor and a few well-separated MTSSL network spins attached to synthetic peptides, accessible by noninvasive optical readout. Our triple-resonance scheme allows us to further extract the coupling between these network spins, which we specifically engineered via molecular chemistry. The demonstrated interface between a well-controllable probe spin and a coupled spin network opens a new venue for realizing a programmable spin network that could allow (i) the transfer of polarization (information) between remote probes, or perform long-distance gates acting as a quantum bus (ii) for a large-scale simulation of solid-state spin Hamiltonians or (iii) for structural analysis of single large proteins using multi electron-electron spectroscopy at the nanoscale. With a continuous microwave driving of the probe, one can polarize the network spins via the double-resonance Hartman-Hahn techniques (36, 37). These polarized spin networks can narrow the linewidth of response on the probes, thus enhancing the fidelity of the network in achieving the targeted goals. In Fig. 4, we plot the expected response on the probe spins for the various protocols described above.

While cryogenic conditions enhance the ability to conduct long-term and highly reproducible electron spin spectroscopy measurements of the targeted molecules, they also assist in implementing projective readout of the probe, adding more quantum features to the control of the network (38). The measured network spin coherence time is close to the limit defined by the hydrogen nuclear spins in the MTSSL environment, and this can be further improved by deuterating the molecule to which the electron spins are attached (39). For generating tunable structures of the network, one can perform lithography to define

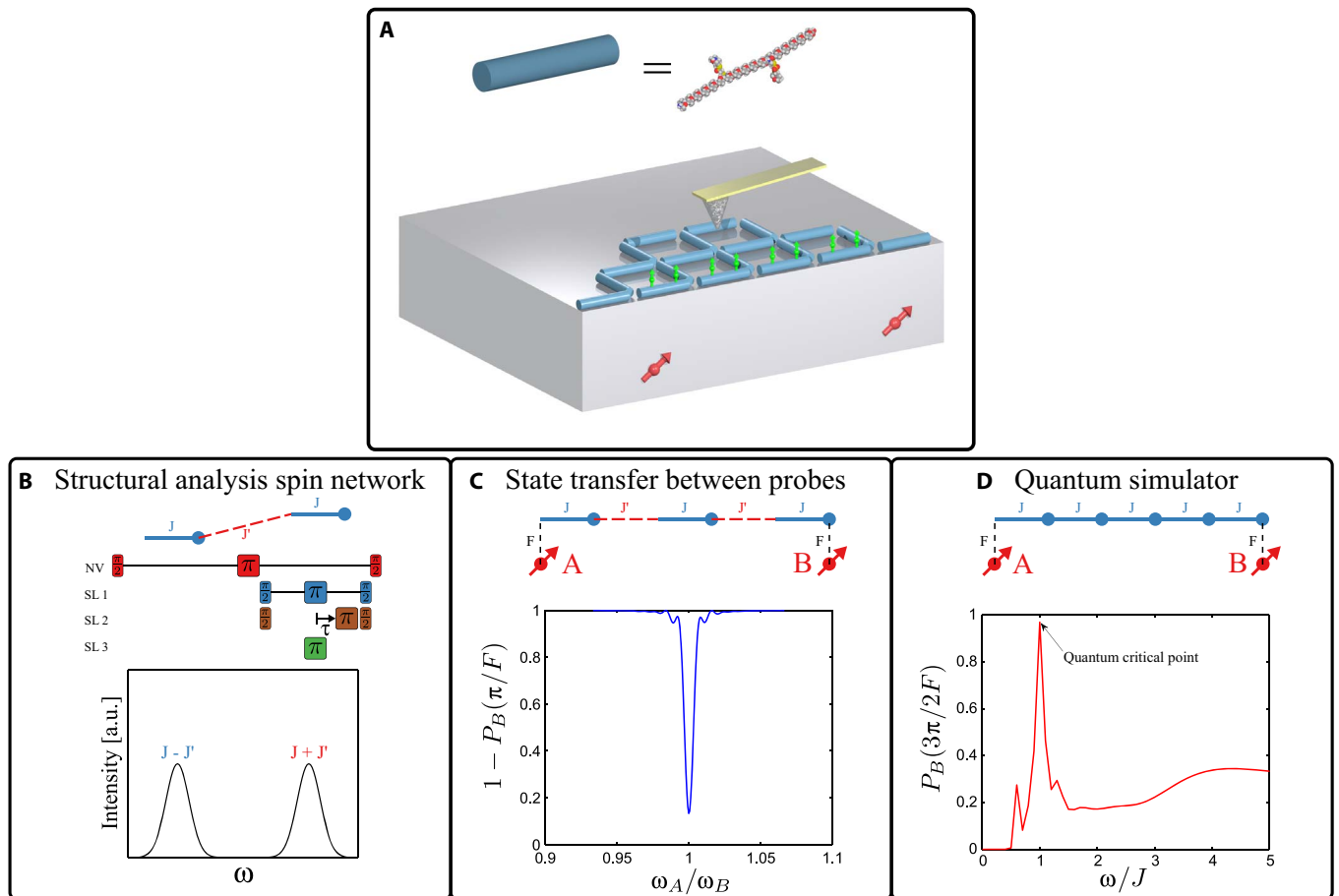


Fig. 4. Schemes for spin network applications. (A) Schematic representation of the envisaged probe-controlled spin network (with intracell and intercell couplings, J and J' , respectively), equipped with an atomic force microscopy magnetic tip to generate gradient fields on nanometer length scales. (B) Extension of the multi-electron spectroscopy to extract intercell couplings, which can further lead to the structural analysis of the spin network. By varying the π pulse time on the second τ , we arrive at the Fourier components of the observed probe spin response. (C) Remote communication between two probes via a spin chain is shown, where the response on the probe spin B , $P_B(t) = \langle S_B^z \rangle$, varies by sweeping the frequency of the probe A . When $\omega_A = \omega_B$, the quantum state of probe A is transferred to B . (D) The effect of the quantum critical point (QCP) in a transverse Ising chain on the state transfer between the two remote probes. At QCP corresponding to $\omega = J$, the fidelity drastically increases—indicating enhanced long-range correlations in the chain.

nanoscale features inhibiting growth in certain regions while binding molecules in others (9). Alternatively, self-assembly of peptides on specific surfaces can be controlled by sequencing and yield well-defined and regular two-dimensional structures (8). The triple-resonance scheme can be generalized to access all elements of the coupling tensor and the interscaffold couplings, J' (see, for example, Fig. 4B). Whereas the electronic spins are used to form the network, the nuclear spins attached to them can act as a memory due to their long lifetime even under ambient conditions. Accessing and manipulating these spins could become helpful in understanding how information flows across a spin network and becomes available to multiple probes simultaneously (Fig. 4C) and also as a probe for unveiling the quantum-critical behavior in a spin network (see Fig. 4D).

MATERIALS AND METHODS

NV double electron-electron resonance spectroscopy

The total Hamiltonian H governing the network spin dynamics is given by the sum of the sensor spin Hamiltonian H_S , the net-

work spin Hamiltonian H_σ , and the sensor-network interaction Hamiltonian $H_{S\sigma}$

$$\begin{aligned} H &= H_S + H_\sigma + H_{S\sigma} \\ H_S &= DS_z^2 + \gamma_S BS_z + \Omega(t)S_x \\ H_\sigma &= \sum_k \gamma_\sigma B \sigma_z^k + A_{zz}^k \sigma_z^k J_z^k + \omega(t) \sigma_x^k + \sum_{kl} \sigma^k \cdot J^{kl} \cdot \sigma^l \\ H_{S\sigma} &= S_z \sum_k F^k \cdot \sigma_z^k \end{aligned} \quad (1)$$

In the above equation, B is the strength of the external magnetic field applied along the quantization axis of the NV center probe spin, with spin operator $S = (S_x, S_y, S_z)$, $S = 1$, and D is its zero-field splitting. The dipolar coupling between the probe spin and the k th network electron spins, with spin operator $\sigma^k = (\sigma_x^k, \sigma_y^k, \sigma_z^k)$, $\sigma = 1/2$, is given by the scalar F^k , and the intracell coupling among the network spins is given by the dipolar coupling tensor J^{kl} . The hyperfine coupling between the network electron spins and their respective nuclear spin environment is denoted by A due to a nearest neighbor ^{14}N nucleus with spin operator $I = (I_x, I_y, I_z)$, $I = 1$. $\Omega(t)$ and $\omega(t)$ are the respective probe and network AC driving

fields. When the Zeeman splitting of the network spins along the field direction is much larger than their internal couplings, one may neglect the nonsecular terms, simplifying the dipolar coupling between the spins to $\sigma^k \cdot J^{kl} \cdot \sigma^l = J_{kl}^{\perp}(\sigma_+^k \sigma_-^l + \sigma_-^k \sigma_+^l) + J_{kl}^{\parallel} \sigma_z^k \sigma_z^l$. Similarly, because of the large difference in the Larmor frequencies between the electron and nuclear spins, the dominant contribution of the hyperfine interaction comes from $A_{zz}^k \cos(\theta_k)$, where θ_k is the relative angle between the external magnetic field and the orientation of the network spins.

The dipolar coupling between the network spins (which are deposited on the surface of the diamond) and the probe results in an additional phase evolution of the probe spin. To observe this phase, one has to decouple the probe spin from the unwanted environmental phase noise. By flipping the probe spin at the midpoint of the decoupling sequence, the random phase accumulated before and after the flip cancels. Thus, to keep the phase information of the network spins, one needs to flip them along with the probe spin such that their contribution to the phase evolution of the probe is not canceled (see Fig. 1B). This procedure, also known as double electron-electron resonance (DEER) sequence, will lead to a contrast (that is, an additional decoherence channel) in the readout of the probe spin as the microwave frequency is swept through the resonance of the network spins. The relative orientation between the molecular frame of the MTSSL network spin and the magnetic field can then be found by rotating the magnetic field away from the quantization axis of the probe. As each MTSSL network spin can have a distinct orientation with respect to the applied field, knowledge of these satellite peaks might allow us to manipulate them individually.

Sample preparation

To achieve close proximity between NV centers and electron spins, we used an electronic grade diamond (Element 6), thinned down to a thickness of 30 μm (Applied Diamond), in which we implanted nitrogen ions at an energy of 5 keV, yielding a mean implantation depth of 7 nm below the diamond surface (40), in a dosage that allows to distinguish single NV centers by standard confocal microscopy. Subsequently, we etched diamond nanopillars into the implanted membrane to increase optical collection efficiency (41).

We selected the nitroxide MTSSL spin label (42) because of the ease of the SDSL process and the well-known spectral behavior (43). The peptide H-AP₁₀CP₁₀CP₁₀-NH₂ was dissolved in 0.1 M tris buffer (pH 7.8) with the addition of 30 mM tris(2-carboxyethyl)phosphine (TCEP) at a concentration of 1 mg/ml. The MTSSL spin label was dissolved in dimethylsulfoxide (0.1 mg/ μl). The peptide (114 nmol) was incubated with MTSSL (5 μmol) overnight at 4°C. The free spin label was removed from the sample by a polyacrylamide desalting column, which was equilibrated with 0.1 M tris buffer (pH 7.8) before the sample was applied to the column. The fractions that contain peptides were concentrated by a Pierce protein concentrator. The spin-labeled peptide was dialyzed in ZelluTrans Mini Dialyzer against water to remove the buffer.

After a standard three-acid (1:1:1 H₂SO₄/HNO₃/HClO₄) treatment on the diamond membrane, to clean and oxygen-terminate the diamond surface, we covered the diamond with a $\sim 3\text{-}\mu\text{l}$ solution of H₂O, which contains $\sim 100\text{ }\mu\text{M}$ peptides in a dropcasting fashion. The diamond was then situated in a nitrogen-rich atmosphere for around 1 hour until all water had evaporated from the solution. This yielded a surface coverage of $\geq 200\text{-nm}$ peptide crystallites. We mounted the diamond membrane on a microwave guide sample holder and spanned a 17- μm gold wire across the surface in close proximity to the NV centers of in-

terest to supply high-power microwave radiation for active manipulation of electronic spins. To conduct an NV center spin-dependent fluorescence readout, we used a home-built confocal microscope that contains both an ambient scanner unit and a unit situated in a UHV environment, which can be cooled down to liquid helium temperatures (34). All experiments were conducted under an external magnetic field of 100 Oe, aligned with the NV axis.

EPR spectroscopy

To infer the size of the polypyrrole molecule, measurement of the dipolar coupling between electron spins on the cysteine sites in a commercial electron paramagnetic resonance (EPR) spectrometer is performed, usually in a frozen deuterated buffer solution, and the distance is subsequently back-calculated. The derived distance distribution between the two cysteine sites on the above-described polypyrrole is around $3.5 \pm 1.0\text{ nm}$ (see the Supplementary Materials) (44, 45). The high error margin is caused here by the fact that these measurements average over billions of molecules and the many resulting geometric conformations. Note that, in this case, it is actually the relative flexibility of the spin label tether that causes the variance in the distance distribution rather than the actual protein conformation itself. Assuming a polypyrrole helix II, the distance between the two cysteine moieties should be around 3.1 nm, as determined by molecular dynamics simulations (29).

Materials

The thiol-specific spin label MTSSL was obtained from Enzo Life Sciences, TCEP was purchased from Sigma-Aldrich, the Pierce protein concentrator PES 3K MWCO and polyacrylamide desalting columns 1.8 K MWCO were obtained from Thermo Fisher Scientific, and the ZelluTrans/Roth Mini Dialyzer MD 300 MWCO 3500 were purchased from Carl Roth.

SUPPLEMENTARY MATERIALS

Supplementary material for this article is available at <http://advances.sciencemag.org/cgi/content/full/3/8/e1701116/DC1>

section S1. Model Hamiltonian
section S2. Modeling of pulse sequences
section S3. Controlling the spin network
section S4. Matrix-assisted laser desorption/ionization (MALDI)
section S5. EPR spectroscopy
section S6. Measurements under ambient conditions
fig. S1. Simulation of the Hamiltonian under DEER spectroscopy.
fig. S2. Simulation of the Hamiltonian under triple electron-electron resonance (TEER) spectroscopy.
fig. S3. MALDI measurement.
fig. S4. Continuous wave (CW) and pulsed EPR measurements.
fig. S5. DEER spectroscopy under ambient conditions.
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Acknowledgments: We thank A. Brunner, T. Häberle, and D. Schmid-Lorch for fruitful discussions. We also thank M. Hagel for assistance in sample preparation, S. A. Momenzadeh for advice in diamond nanofabrication, and S. Rauschenbach for help with peptide mass spectrometry. We acknowledge financial support from the European Union via grant no. 611143 (DIADEMS) and the Deutsche Forschungsgemeinschaft via SPP 1601 and Research Group 1493. F.F.d.O. acknowledges CNPq (Conselho Nacional de Desenvolvimento Científico e Tecnológico) for the financial support through project no. 204246/2013-0. A.F. acknowledges financial support from the Alexander von Humboldt Foundation. **Author contributions:** L.S., T.O., A.F., and J.W. conceived the experiment. L.S., K.X., B.K., and T.O. performed the NV measurements. A.Z., M.A., and M.D. prepared the samples. M.A. performed the ESR spectrometer measurements. F.F.d.O. prepared the diamond membrane with NV centers, and A.F. fabricated nanopillars on it. L.S., D.B.R.D., and A.F. analyzed the data and wrote the manuscript with input from all authors. M.T., K.K., J.W., and A.F. supervised the project. **Competing interests:** The authors declare that they have no competing interests. **Data and materials availability:** All data needed to evaluate the conclusions in the paper are present in the paper and/or the Supplementary Materials. Additional data related to this paper may be requested from the authors.

Submitted 10 April 2017

Accepted 12 July 2017

Published 11 August 2017

10.1126/sciadv.1701116

Citation: L. Schlipf, T. Oeckinghaus, K. Xu, D. B. R. Dasari, A. Zappe, F. F. de Oliveira, B. Kern, M. Azarkh, M. Drescher, M. Ternes, K. Kern, J. Wrachtrup, A. Finkler, A molecular quantum spin network controlled by a single qubit. *Sci. Adv.* **3**, e1701116 (2017).

A molecular quantum spin network controlled by a single qubit

Lukas Schlipf, Thomas Oeckinghaus, Kebiao Xu, Durga Bhaktavatsala Rao Dasari, Andrea Zappe, Felipe Fávaro de Oliveira, Bastian Kern, Mykhailo Azarkh, Malte Drescher, Markus Ternes, Klaus Kern, Jörg Wrachtrup and Amit Finkler

Sci Adv **3** (8), e1701116.
DOI: 10.1126/sciadv.1701116

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